

# Quantitative neuroimaging in multiple sclerosis

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# Overview



## Background

Relevance, 'MRI quantification' approaches, overview of Radiomics approach



## Objectives

Hypothesis and objectives



## Materials and methods

Data description, MRI processing pipeline, analysis pipeline



## Results

Models internal and external validation



## Conclusion

Current results + future study

# Background

## Multiple sclerosis



### 'Disease assessment'

Important for personalized medicine



### Multiple sclerosis

Heterogeneity and lack of pathognomonic signs



### Pathological changes

Brain tissues demyelination and inflammation



### MRI

Non-invasive, 3D, repeatable, with corresponding contrast

# Background

What is MRI signal?



**MRI 'measurements'**  
Properties of H atoms

**H nucleus**

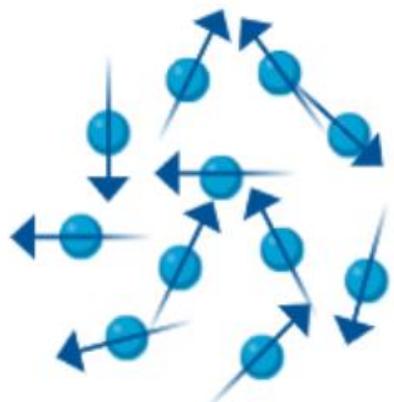
- spinning charged particle
- produces magnetic field = magnetic moment

**In external magnetic field**  
Magnetic moment precession (Larmor precession)

$$\omega = -\gamma B$$

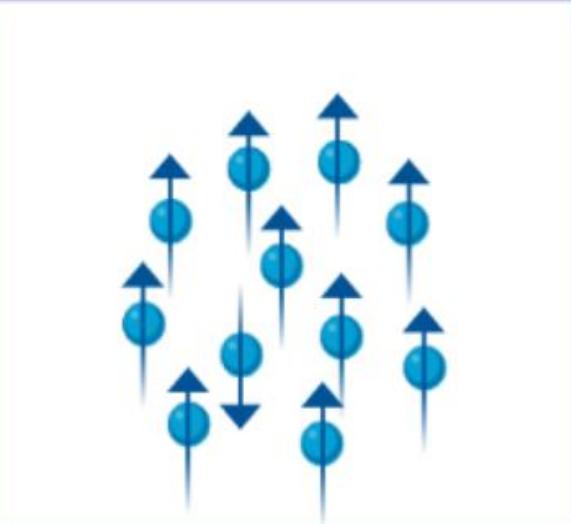
# Background

What is MRI signal?



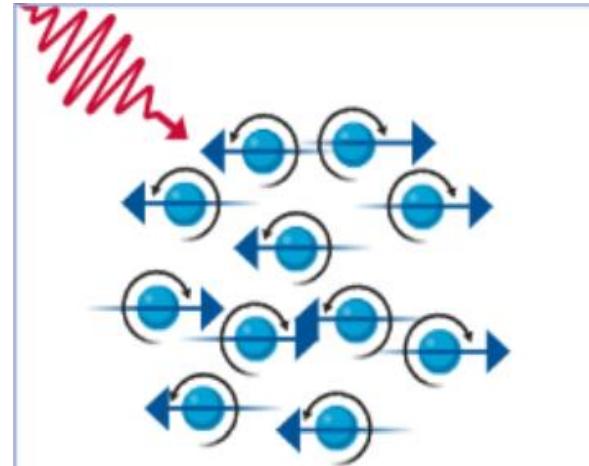
**No magnetic field**

Spins randomly positioned



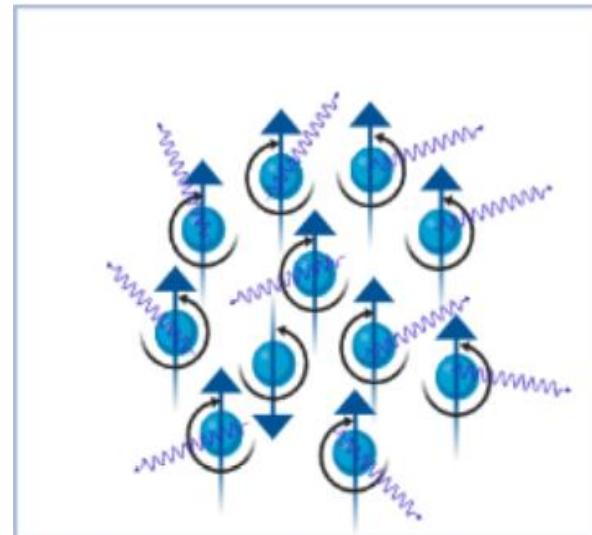
**Constant magnetic field**

Spins mostly aligned



**Radio pulse**

- Longitudinal magnetization ↓
- Transversal magnetization ↑



**Protons relax**

Radiosignal released

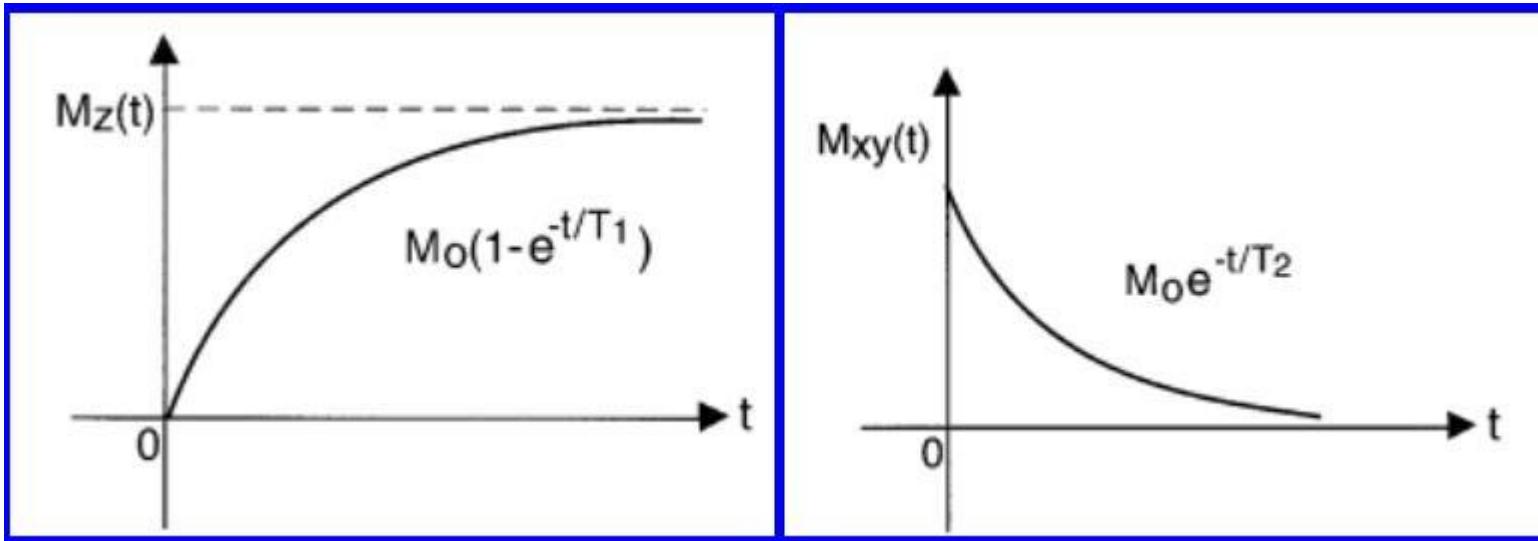
Relaxation measured in longitudinal and transversal directions

**Z**

**X**

# Background

What is MRI signal?



## Longitudinal relaxation

Spin-lattice  
Towards thermal equilibrium  
Characterized by  $T_1$

## Transversal relaxation

Spin-spin  
Out of phase  
Characterized by  $T_2$

(in reality)

$T_2$  = real value

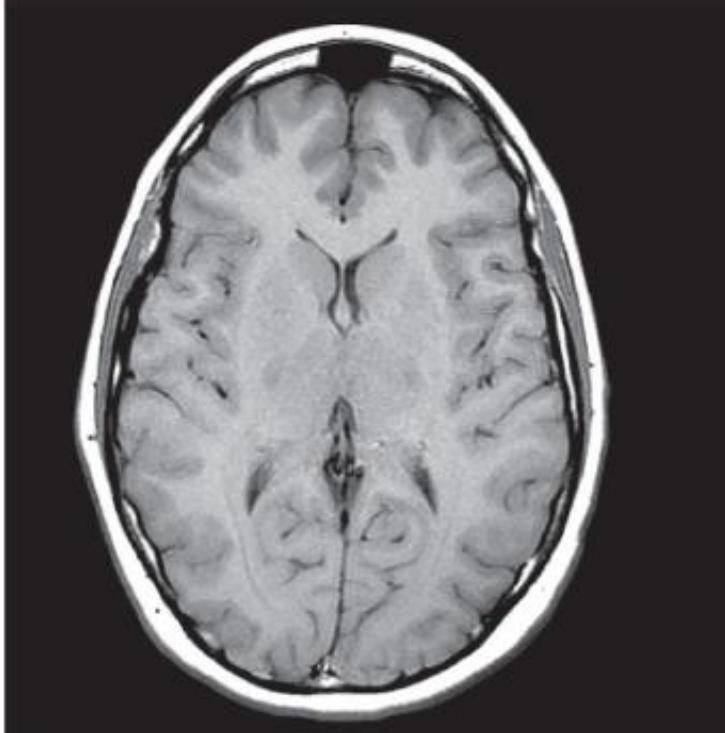
$T_2^*$  = observer value

$T_2^* < T_2$

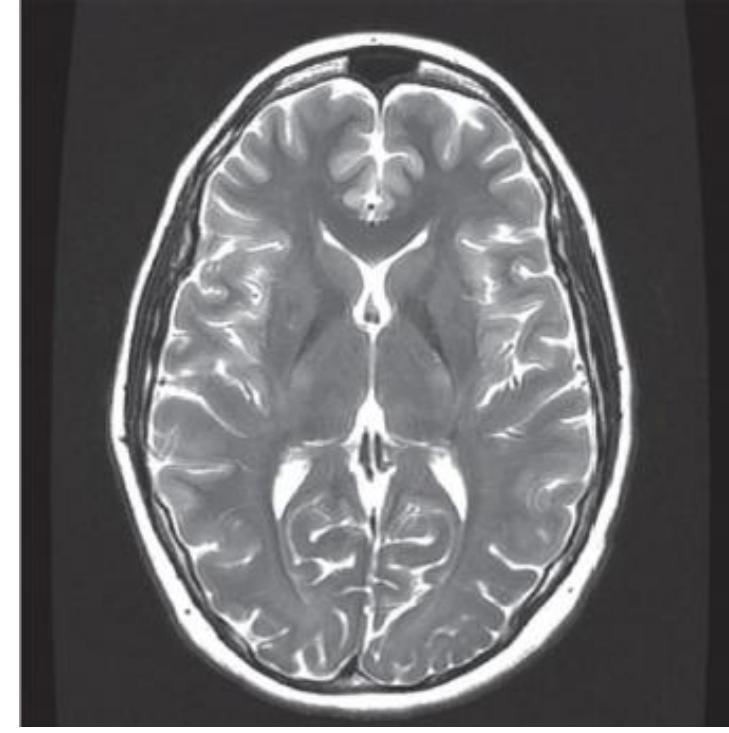
$$\frac{1}{T_2^*} = \frac{1}{T_2} + \frac{1}{T_{2inhom}}$$

# Background

What is MRI signal?



T1w



T2w

# Background

What is MRI signal?

No ionizing radiation

Can visualize 'any' structure, playing with sequences

Expressed in arbitrary units → good for visual analysis only

Low reproducibility across centers, vendors, scanners, protocols, etc

**Objective reproducible MRI-based analysis is required!**

# Background

## 'MRI quantification' approaches

NeuroImage: Clinical 23 (2019) 101879

Contents lists available at ScienceDirect

**NeuroImage: Clinical**

journal homepage: [www.elsevier.com/locate/ynicl](http://www.elsevier.com/locate/ynicl)

**Multiparameter MRI quantification of microstructural tissue alterations in multiple sclerosis**

Emilie Lommers<sup>a,b,\*</sup>, Jessica Simon<sup>c</sup>, Gilles Reuter<sup>a,d</sup>, Gaël Delrue<sup>b</sup>, Dominique Dive<sup>b</sup>, Christian Degueldre<sup>a</sup>, Evelyne Balteau<sup>a</sup>, Christophe Phillips<sup>a,e</sup>, Pierre Maquet<sup>a,b</sup>

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<sup>b</sup> Clinical Neuroimmunology Unit, Neurology Department, CHU Liège, Belgium  
<sup>c</sup> Psychology and Neurosciences of Cognition Research Unit, University of Liège, Belgium  
<sup>d</sup> Neurosurgery Department, CHU Liège, Belgium  
<sup>e</sup> GIGA – *in silico* Medicine, University of Liège, Liège, Belgium

### MRI quantitative multi-parameter mapping (qMRI)

Liege University

### Radiomics

Maastricht University

Review Article | Published: 04 October 2017

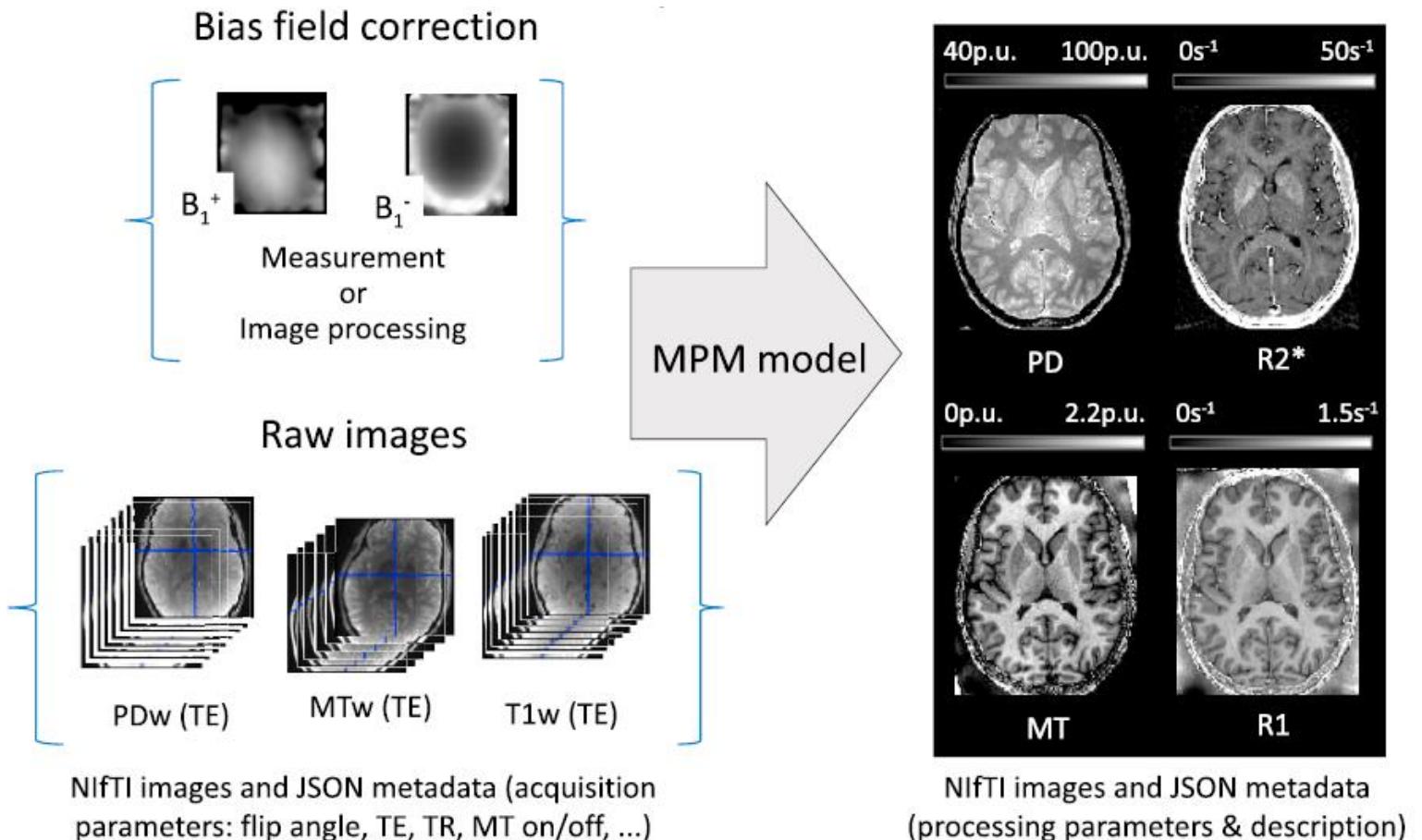
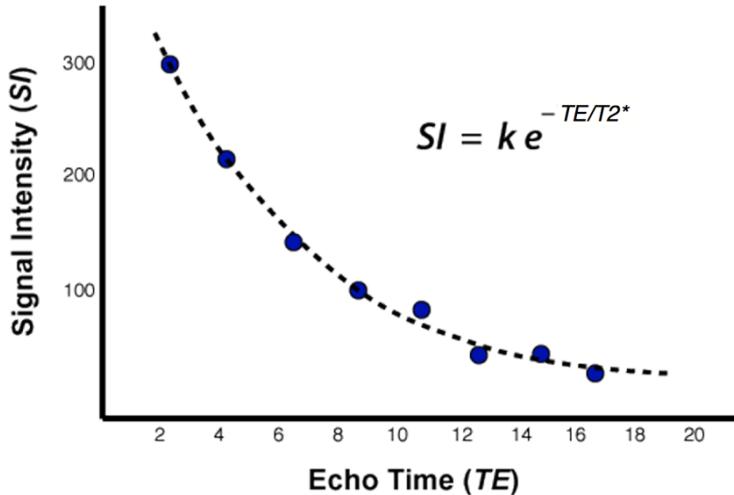
### Radiomics: the bridge between medical imaging and personalized medicine

Philippe Lambin , Ralph T.H. Leijenaar, Timo M. Deist, Jurgen Peerlings, Evelyn E.C. de Jong, Janita van Timmeren, Sebastian Sanduleanu, Ruben T.H.M. Larue, Aniek J.G. Even, Arthur Jochems, Yvonka van Wijk, Henry Woodruff, Johan van Soest, Tim Lustberg, Erik Roelofs, Wouter van Elmpet, Andre Dekker, Felix M. Mottaghy, Joachim E. Wildberger & Sean Walsh

*Nature Reviews Clinical Oncology* **14**, 749–762 (2017) | Download Citation 

# Background

## What is qMRI?



# Background

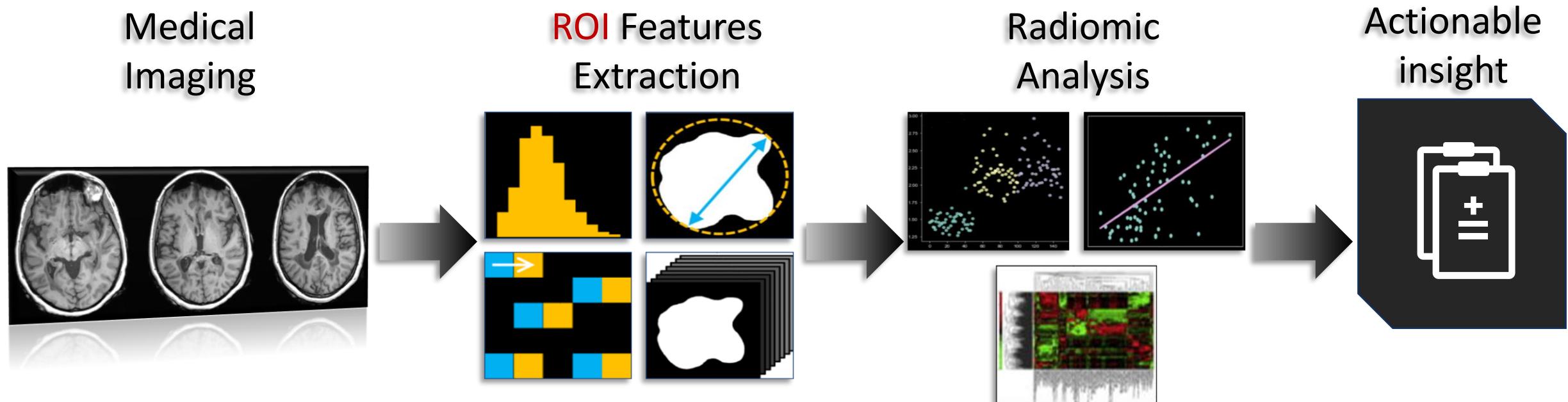
What is qMRI?

Map	Name	Possible biological interpretation	Units
PD	Proton density	Free water	%
MT	Magnetization transfer saturation	Axonal myelination	%
R1	Longitudinal relaxation time	Axonal myelination	Hz
R2*	Transverse relaxation time	Iron accumulation	Hz

quantitative, in physical units

# Background

## Radiomics pipeline



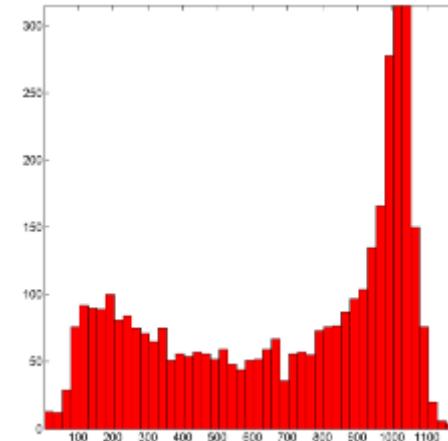
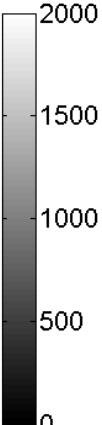
# Background

Radiomics feature classes

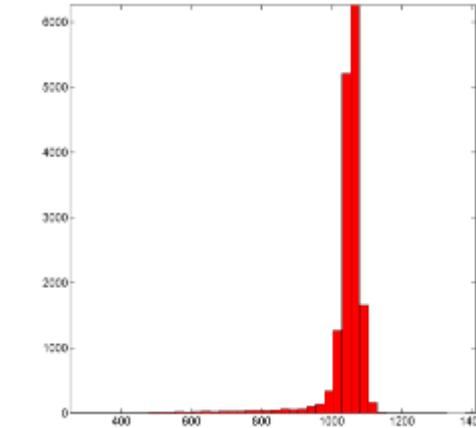
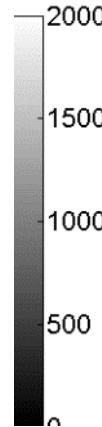
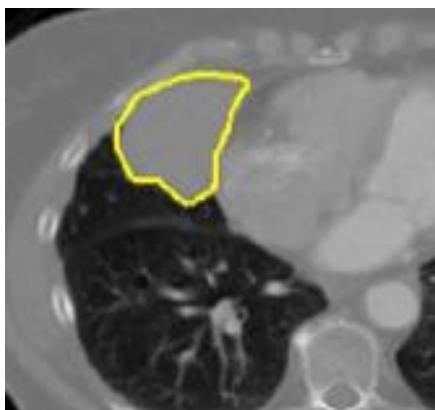


# Background

## Radiomics feature example: Tumour intensity



Minimum	4
Maximum	1180
Mean	687,13
Range	1176
Standard deviation	336,51
Variance	113237,17
Median	799
Skewness	-0,46
Kurtosis	1,70
Entropy	6,49
RMS	765,08
Total energy	6432571,20
Mean deviation	302,00

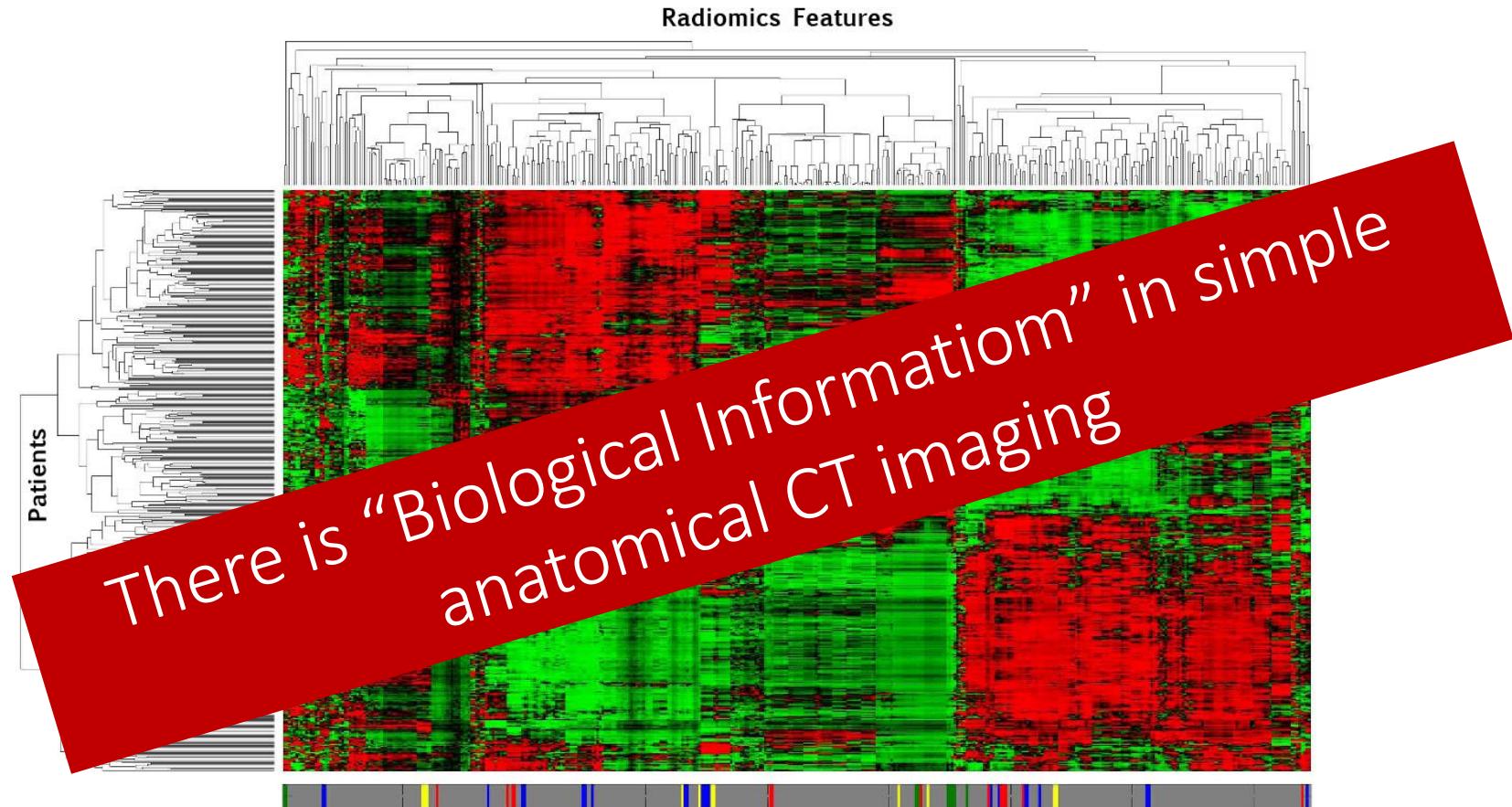


Minimum	254
Maximum	1411
Mean	1043,75
Range	1157
Standard deviation	65,78
Variance	4327,46
Median	1055
Skewness	-5,18
Kurtosis	37,88
Entropy	3,58
RMS	1045,82
Total energy	49141473,18
Mean deviation	30,63

Lambin et al. EJC, 2012;; Lambin et al. Nat Rev Clin Oncol 2017

# Background

## Rationale



Significant association with histology ( $p$ -value = 0.003): *squamous cell carcinoma*, as opposed to *adenocarcinomas*, showed a higher presence in cluster II.

# Objectives

## Hypothesis and objectives

### Hypothesis

Radiomics features, extracted from MS PA and HS MRI, show significant differences in distributions

qMRI improves Radiomics analysis

Radiomics could be used to rapidly diagnose MS on routine MR

Radiomics features contain information about pathological biological processes

### Objectives

To create Radiomics signatures of pathological and healthy brain tissue

To compare conventional MRI- and qMRI-based Radiomics analysis results

To investigate ability of Radiomics models to differentiate between MS PA and HS

To perform early diagnostics of MS, based on qMRI and Radiomics approaches

# Materials and methods

## Data

	T1w + qMRI (PD, MT, R1, R2*)	T1w	T1w
Dataset	Private CHU, Liege, dataset	CC-359	MICCAI 2016 MSSEG challenge dataset
Subjects	MS patients (36), HCS (37)	HCS (359)	MS patients (15)
Sites	CHU, Liege, Belgium; GIGA-CRC in vivo imaging, University of Liege, Liege, Belgium	from Campinas, Sao Paulo, Brazil; Calgary, Alberta, Canada	CHU Rennes, Rennes, France; CHU Lyon, Lyon, France
Equipment	3 T Siemens Magnetom Allegra; 3 T Siemens Magnetom Prisma	1.5 T and 3 T Siemens, Philips, GE Healthcare MRI scanners	3 T Siemens Magnetom Verio; 1.5 T Siemens Magnetom Aera; 3 T Philips Ingenia
Age, $\mu \pm \sigma$ , years	$45.7 \pm 11.9$	$53.5 \pm 7.8$	$41.6 \pm 9.8$
Gender balance, M/F	0.73	0.96	0.88

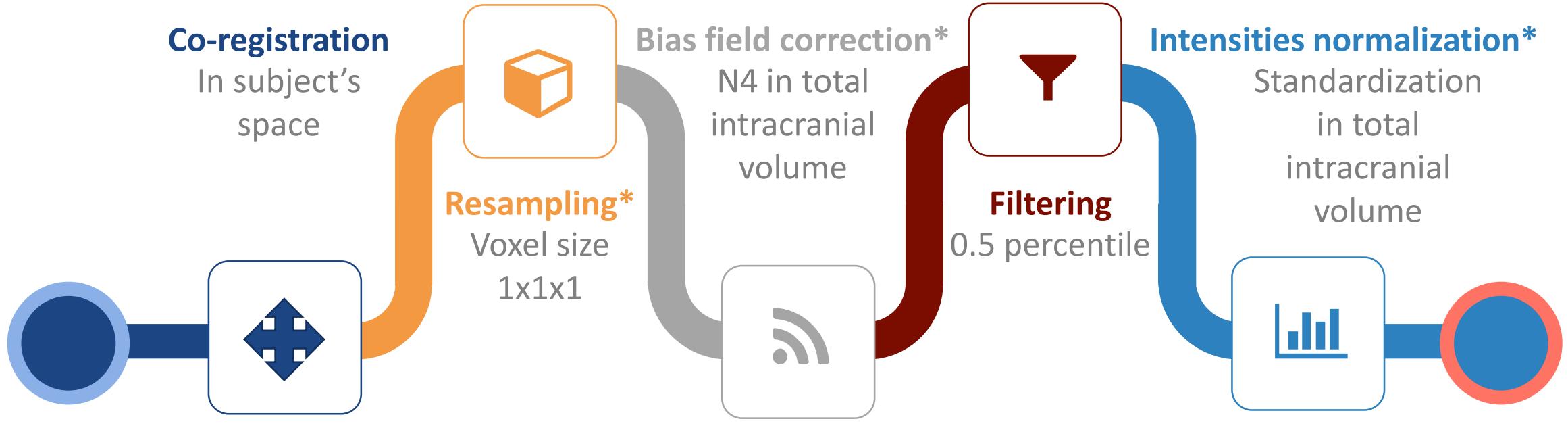
Lommers, et al. (2019). Multiparameter MRI quantification of microstructural tissue alterations in multiple sclerosis. *NeuroImage: Clinical*, 101879.

Souza, et al. (2018). An open, multi-vendor, multi-field-strength brain MR dataset and analysis of publicly available skull stripping methods agreement. *NeuroImage*, 170, 482-494

Commowick, et al. (2018). Objective evaluation of multiple sclerosis lesion segmentation using a data management and processing infrastructure. *Scientific reports*, 8(1), 13650.

# Materials and methods

## MRI preprocessing



\* For conventional MRI only

**DS1**  
Segmentation provided  
Performed with qMRI toolbox

**DS2**  
Segmentation provided  
Consensus of methods

**DS3**  
Segmentation of only lesions maps provided  
Performed with SPM

# Materials and Methods

## Radiomics features extraction



From total WM



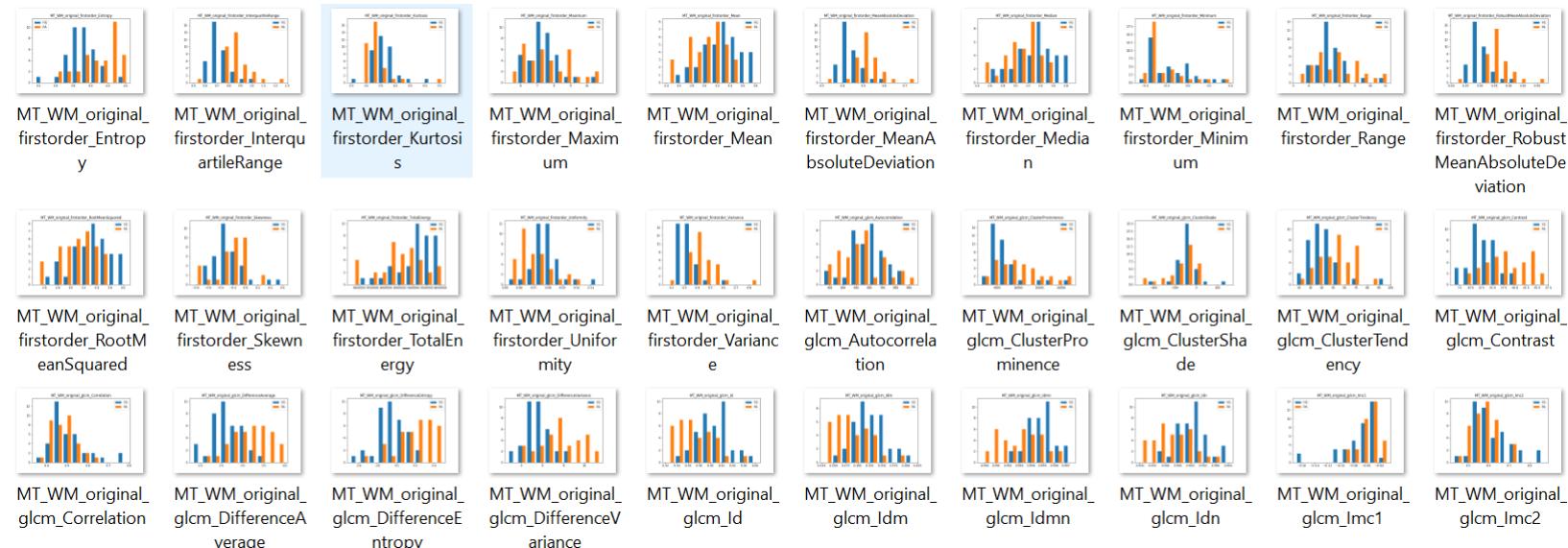
PyRadiomics toolbox



107 features/ROI: intensity, shape, texture (GLCM, GLRLM, GLSJM, GLDM, NGTDM)



Fixed number (50) of greyscale levels in texture analysis



# Materials and methods

## Features selection

### Redundancy

Removing  
intercorrelated  
features

### 'Informativeness'

Mann-Whitney test  
ANOVA F-test  
Model filling (RFC)

### 'Predictiveness'

Recursive features  
elimination

### Robustness

Bootstrapping

For each image type (T1w, PD, MT, R1, R2\* + for mixed qMRI), 5 best features are selected

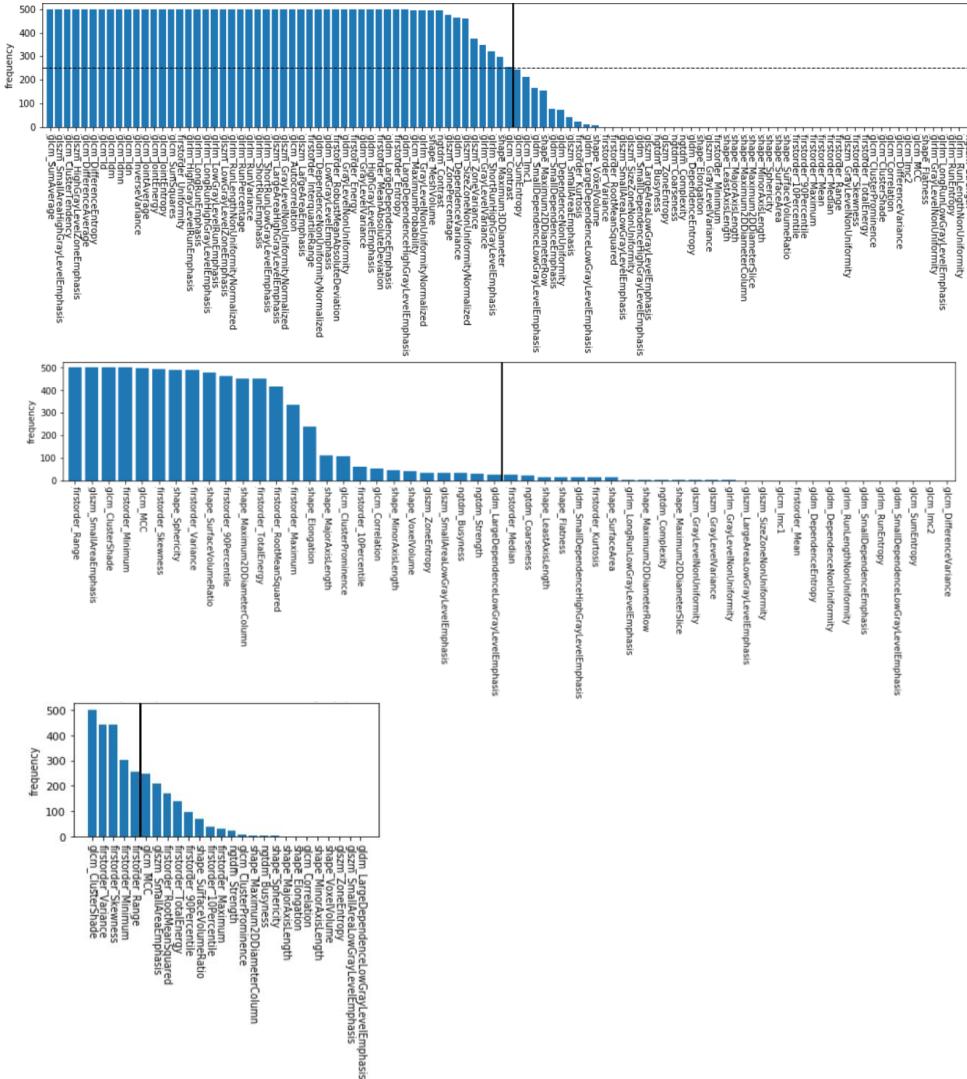
## Materials and methods

## Features selection

# Removing intercorrelated features

## Selecting ‘important’ features (Mann-Whitney test, RFC model fitting, F-test)

## Selecting the best performing features with RFE



# Materials and methods

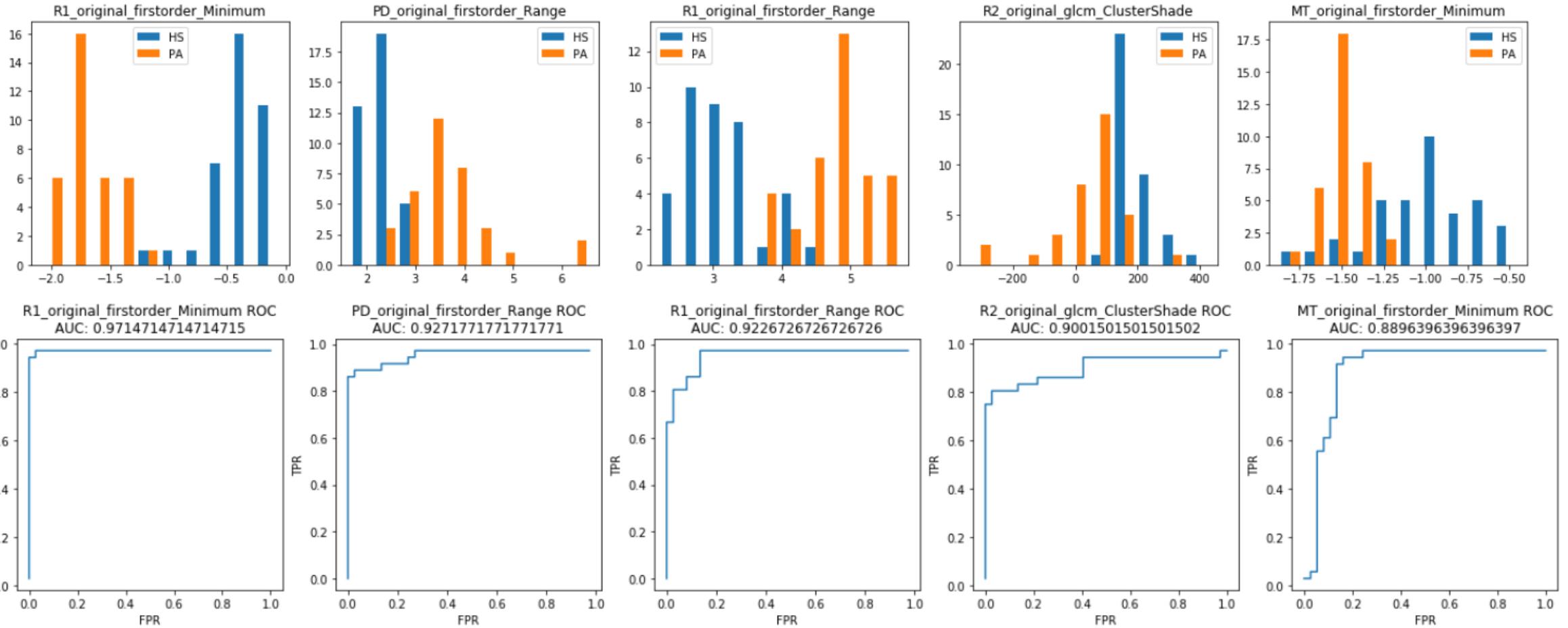
## Features to model

T1	'glcm_ClusterShade', 'firstorder_Variance', 'firstorder_Skewness', 'firstorder_Minimum', 'firstorder_Range'
MT	'firstorder_Minimum', 'firstorder_10Percentile', 'firstorder_Range', 'firstorder_Kurtosis', 'firstorder_RobustMeanAbsoluteDeviation'
PD	'firstorder_Range', 'firstorder_Skewness', 'firstorder_Variance', 'gldm_SmallDependenceHighGrayLevelEmphasis', 'glcm_MCC'
R1	'firstorder_Range', 'firstorder_Minimum', 'firstorder_Skewness', 'firstorder_Kurtosis', 'gldm_LargeDependenceHighGrayLevelEmphasis'
R2*	'gldm_SmallDependenceLowGrayLevelEmphasis', 'firstorder_Skewness', 'glcm_ClusterShade', 'ngtdm_Busyness', 'shape_SurfaceVolumeRatio'
qMRI	'R1_firstorder_Minimum', 'PD_firstorder_Range', 'R1_firstorder_Range', 'R2_glcm_ClusterShade', 'MT_firstorder_Minimum'

*Not correlated to volume!*

# Materials and methods

## Features to model



# Materials and methods

## Classification MS vs non-MS

*Training – with DS1*

	T1w	PD	MT	R1	R2*	mixed qMRI
<b>RFC</b>	CV/EV	CV	CV	CV	CV	CV
<b>SVC</b>	CV/EV	CV	CV	CV	CV	CV
<b>LRC</b>	CV/EV	CV	CV	CV	CV	CV

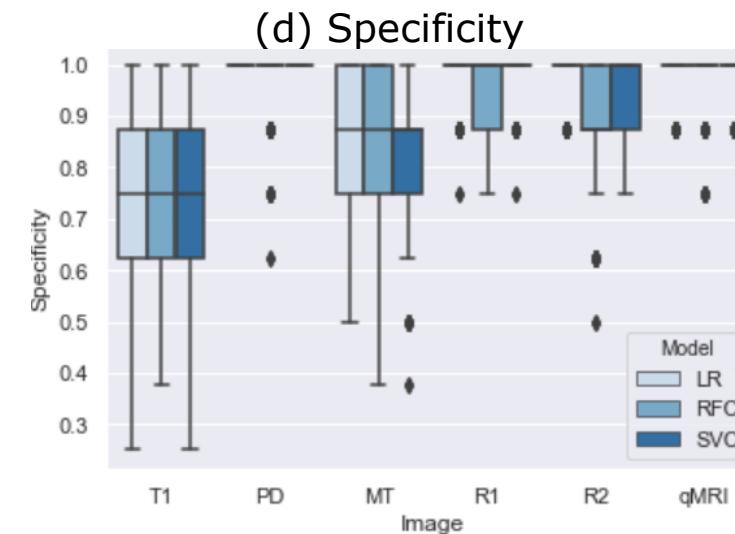
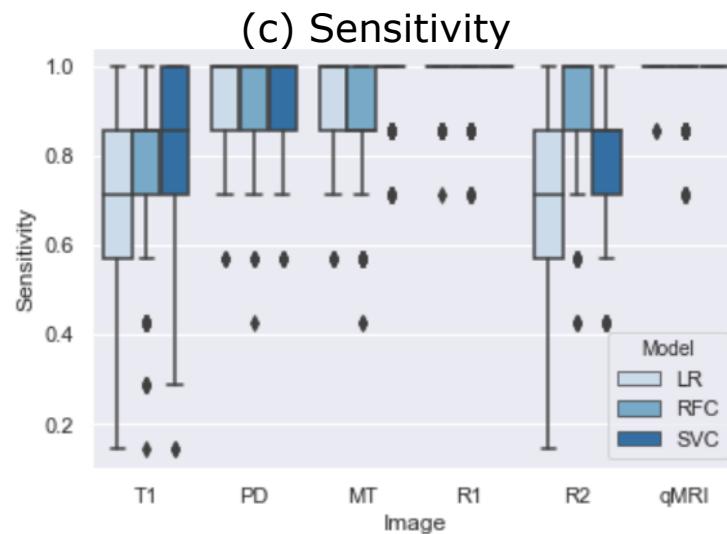
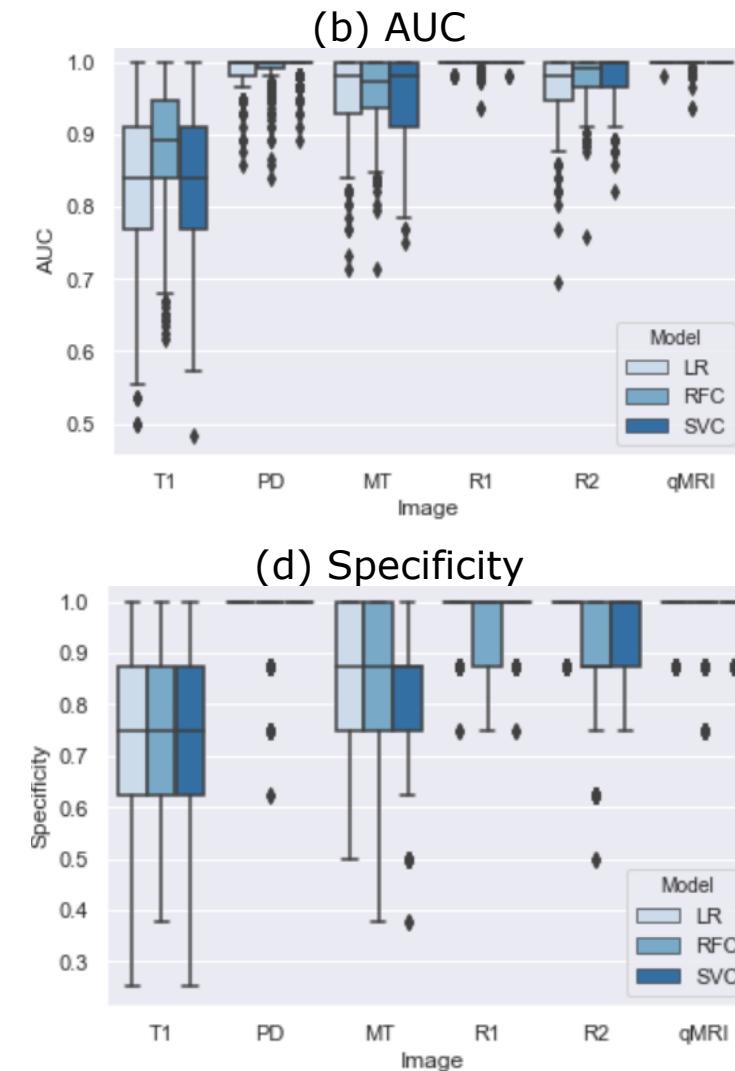
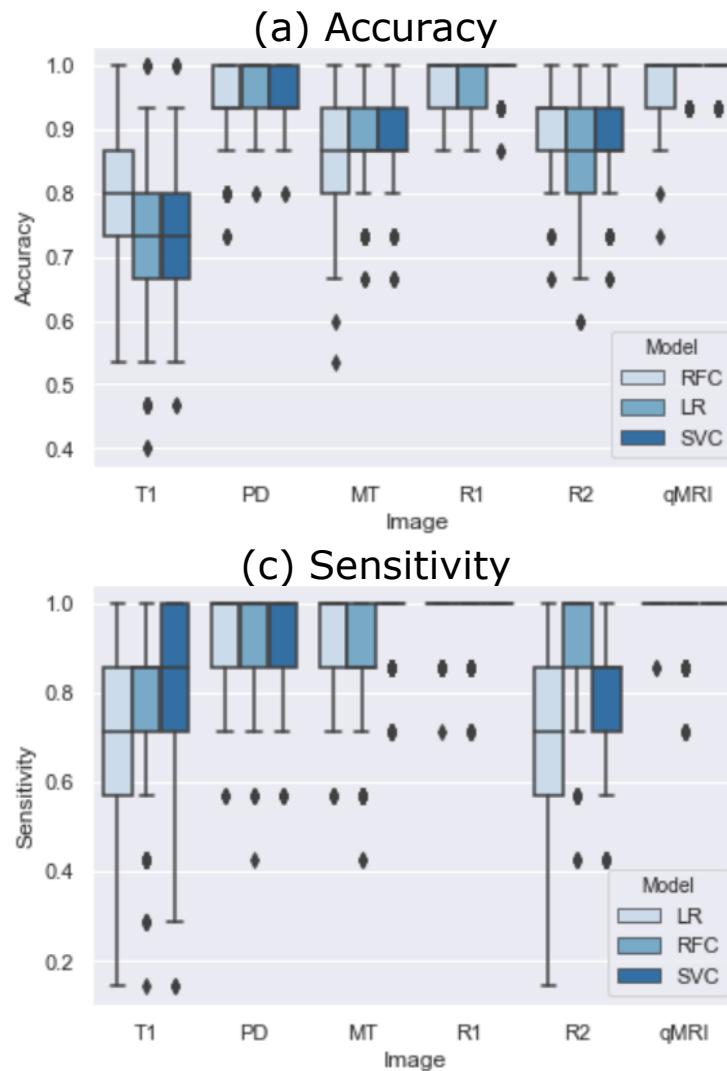
*CV – internal cross-validation with DS1*

*EV – external validation with DS2 and DS3*

\*RFC – Random Forest Classifier, SVC – Support Vector Classifier, LRC – Logistic Regression Classifier

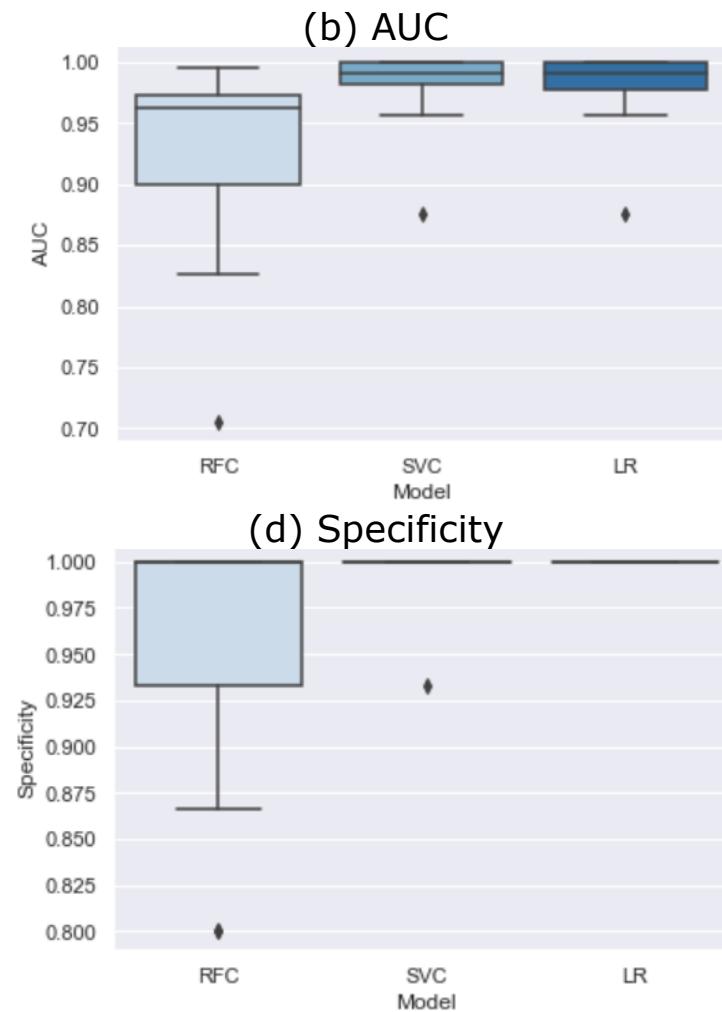
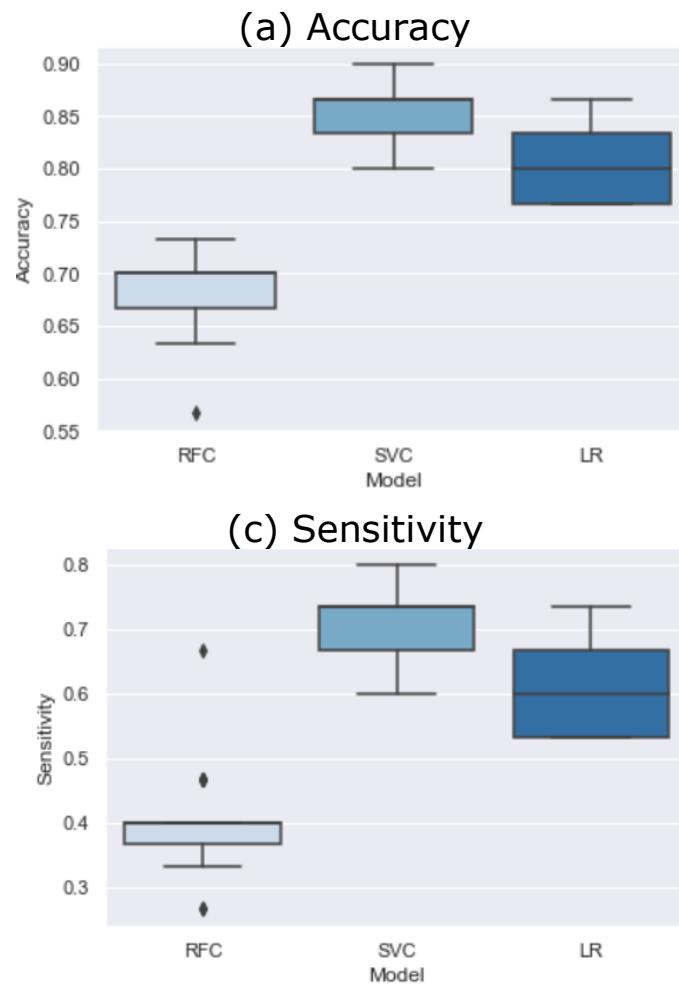
# Results

## Models testing



# Results

## Models validation on external data



DS2 is splitted for classification data balance

# Results

(further work: NAWM AUCs)

	T1w	PD	MT	R1	R2*	qMRI
<b>RFC</b>	0.81 (+/-0.21)	0.92 (+/-0.13)	0.89 (+/-0.16)	0.90 (+/-0.15)	0.82 (+/-0.19)	0.94 (+/-0.12)
<b>SVC</b>	0.79 (+/-0.22)	0.88 (+/-0.19)	0.90 (+/-0.16)	0.87 (+/-0.15)	0.79 (+/-0.20)	0.94 (+/-0.11)
<b>LRC</b>	0.77 (+/-0.22)	0.90 (+/-0.16)	0.91 (+/-0.15)	0.87 (+/-0.18)	0.80 (+/-0.21)	0.95 (+/-0.11)

## Feature groups to model

T1w	GlcM, firstorder, glszm, gldm, firstorder,
PD	Gldm, glcm, glcm, firstorder, glrlm
MT	GlcM, glcm, glcm, glcm, gldm
R1	Firstorder, firstorder, firstorder, gldm, glcm
R2*	Ngtdm, glszm, glszm, glszm, gldm

# Conclusion

## MS RADIOMICS FEATURES VECTORS

The best 5 features are selected for each image type (T1, PD, MT, R1, R2\*):

- not correlated to volume,
- not shape features,
- are understandable and interpretable

## PRELIMINARY CLASSIFICATION MODELS

- Fully automated pipeline
- qMRI perform better on teaching data,
- External validation for qMRI is needed

## EXTERNAL VALIDATION

T1w-based models are validated on external data, performance is comparable to shown on teaching data

## FURTHER STUDY

- Another tissues study
- Another diagnosis study
- Aging study

## 'TECHNICAL TASKS'

- Brain tissues segmentation
- Image quality assessment and preprocessing



**LIÈGE université**  
**GIGA**  
**CRC In vivo Imaging**



**Maastricht University**



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