NeuroImaging Data Processing

aka. Statistical Parametric Mapping short course

Course 5:

Evoked response fMRI & Design efficiency



Christophe Phillips



Content

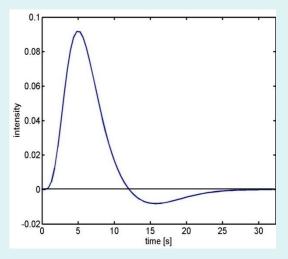
- Block/epoch vs. event-related fMRI
- (Dis)Advantages of efMRI
- GLM: Convolution
- BOLD impulse response
- Temporal Basis Functions
- Timing Issues
- Design Optimisation "Efficiency"

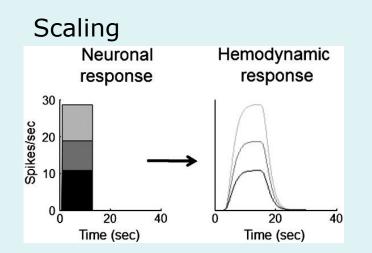
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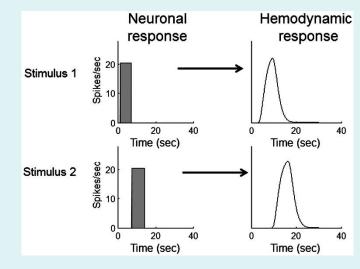
BOLD response

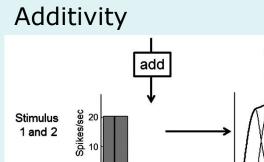
Hemodynamic response function (HRF):





Shift invariance





20

Time (sec)

40

0

40

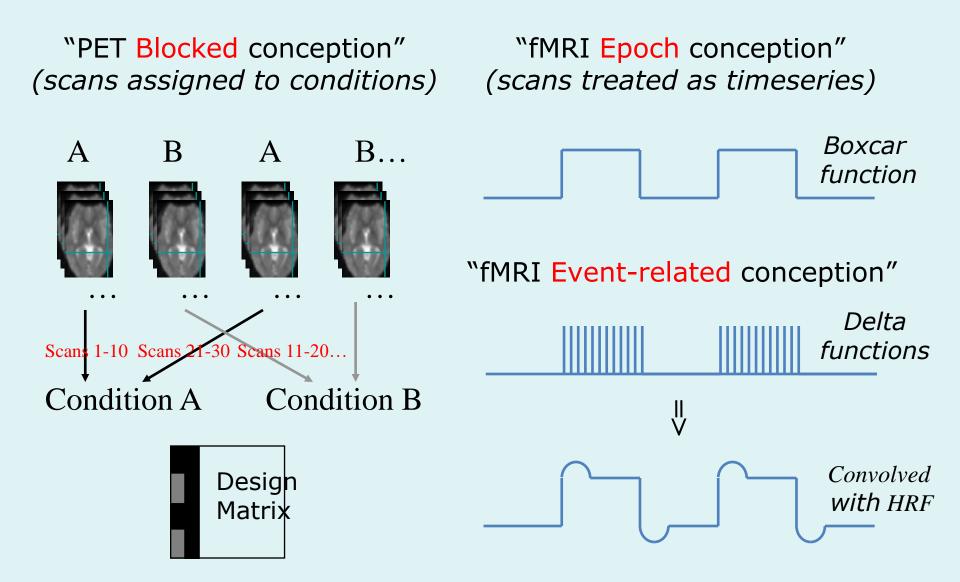
add

20

Time (sec)

0

Epoch vs. event related design



• Randomised trial order *c.f. confounds of blocked designs* Blocked designs may trigger expectations and cognitive sets



Unpleasant (U)

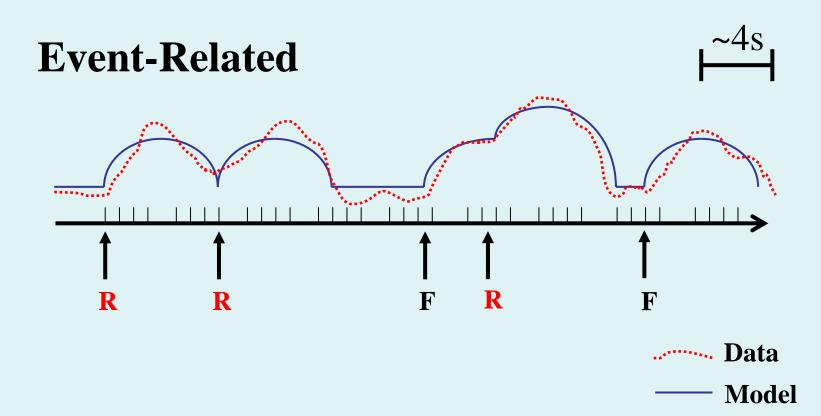
Pleasant (P)

Intermixed designs can minimise this by stimulus randomisation

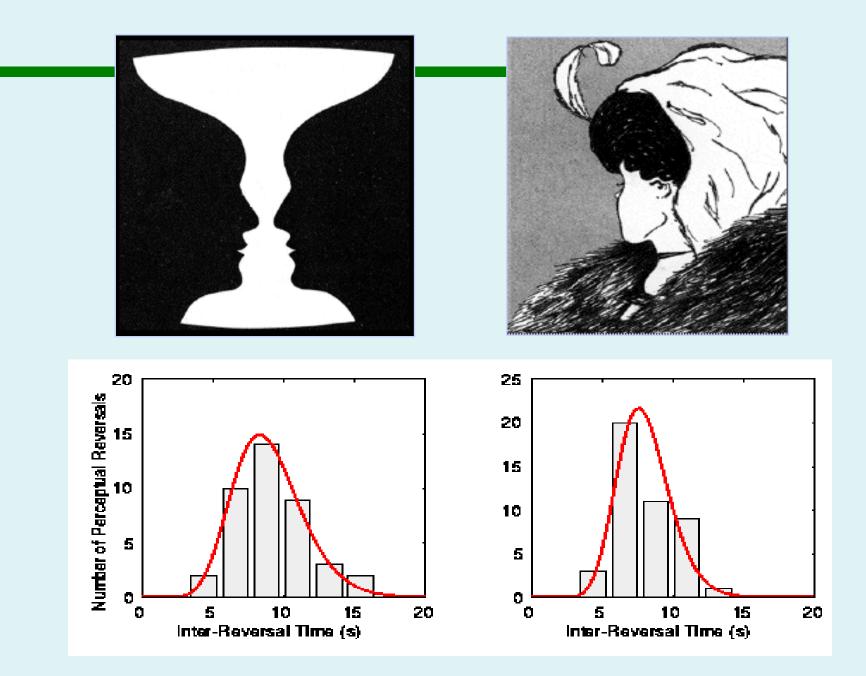


- Randomised trial order c.f. confounds of blocked designs
- Post hoc / subjective classification of trials *e.g, according to subsequent memory*

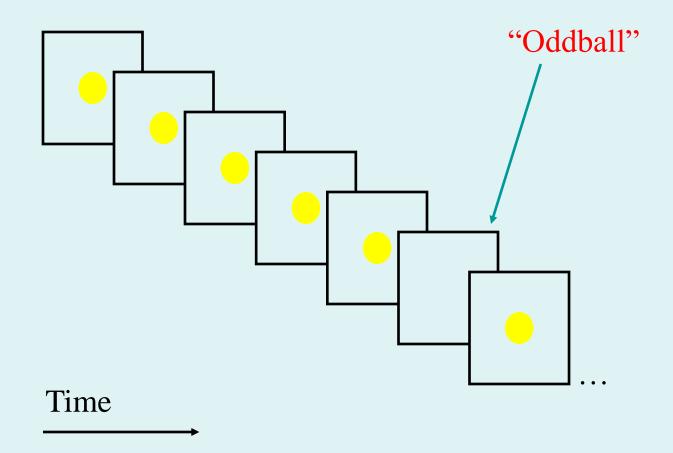
R = Words Later Remembered F = Words Later Forgotten



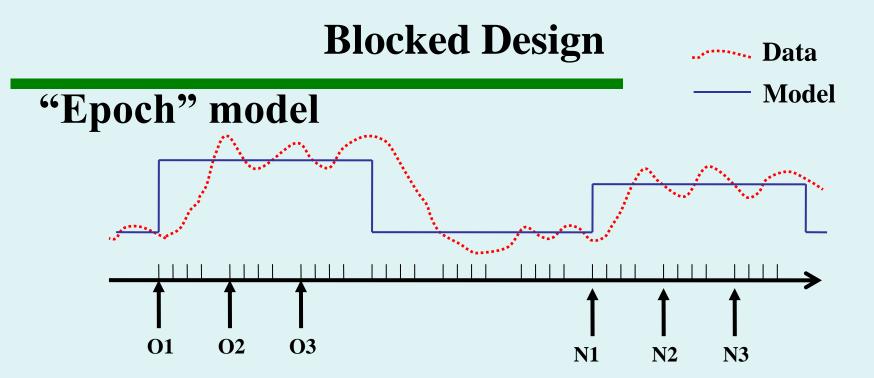
- Randomised trial order *c.f. confounds of blocked designs*
- Post hoc / subjective classification of trials *e.g, according to subsequent memory*
- Some events can only be indicated (in time) e.g, spontaneous perceptual changes



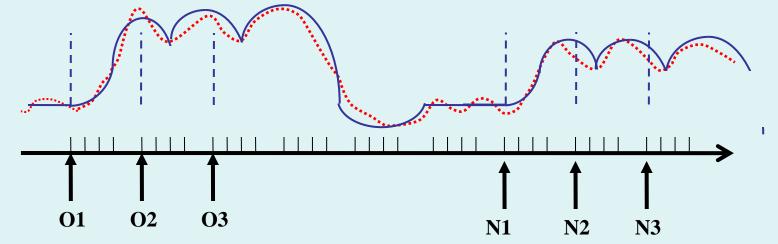
- Randomised trial order *c.f. confounds of blocked designs*
- Post hoc / subjective classification of trials *e.g, according to subsequent memory*
- Some events can only be indicated (in time) e.g, spontaneous perceptual changes
- Some trials cannot be blocked e.g, "oddball" designs



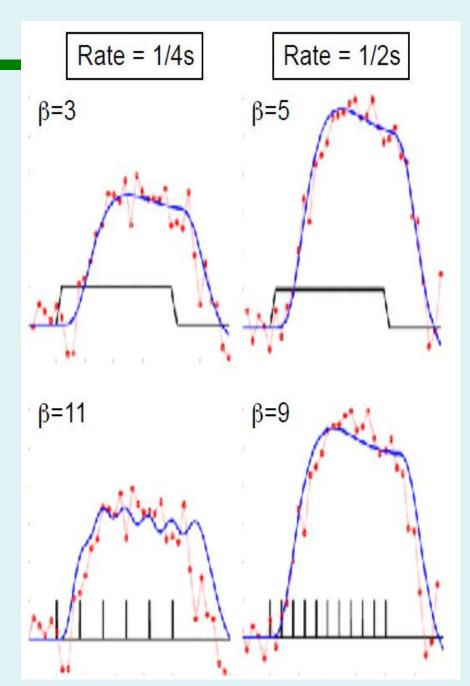
- Randomised trial order *c.f. confounds of blocked designs*
- Post hoc / subjective classification of trials *e.g, according to subsequent memory*
- Some events can only be indicated (in time) e.g, spontaneous perceptual changes
- Some trials cannot be blocked *e.g, "oddball" designs*
- More accurate models even for blocked designs? e.g, "state-item" interactions



"Event" model



- Blocks of trials can be modeled as boxcars or runs of events
- BUT: interpretation of the parameter estimates may differ
- Consider an experiment presenting words at different rates in different blocks:
 - An "epoch" model will estimate parameter that increases with rate, because the parameter reflects response per block
 - An "event" model may estimate parameter that decreases with rate, because the parameter reflects response per word



Disadvantages of ER designs

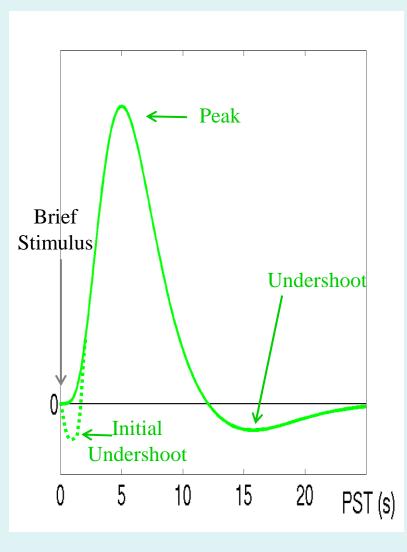
- Less efficient for detecting effects than are blocked designs (see later...)
- Some psychological processes may be better blocked (e.g. task-switching, attentional instructions)

Content

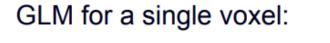
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Haemodynamic response function

- Function of blood oxygenation, flow, volume (Buxton et al, 1998)
- Peak (max. oxygenation)
 4-6s poststimulus; baseline
 after 20-30s
- Initial undershoot can be observed (Malonek & Grinvald, 1996)
- Similar across V1, A1, S1...
- ... but differences across: other regions (Schacter et al 1997) and individuals (Aguirre et al, 1998)



General Linear (Convolution) Model



 $y(t) = u(t) \otimes h(\tau) + \varepsilon(t)$

u(t) = neural causes (stimulus train)

 $u(t) = \sum \delta (t - nT)$

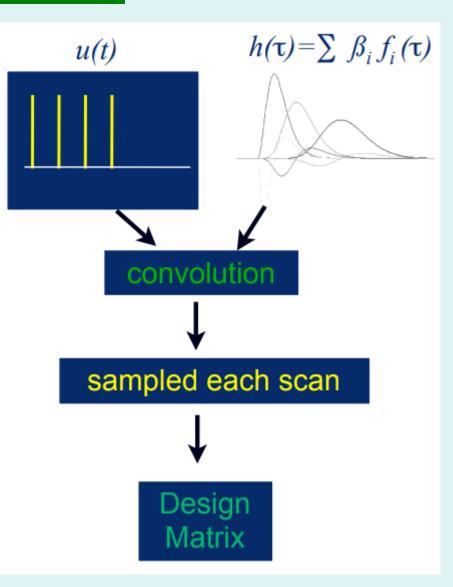
 $h(\tau)$ = hemodynamic (BOLD) response

 $h(T) = \sum B_i f_i(T)$

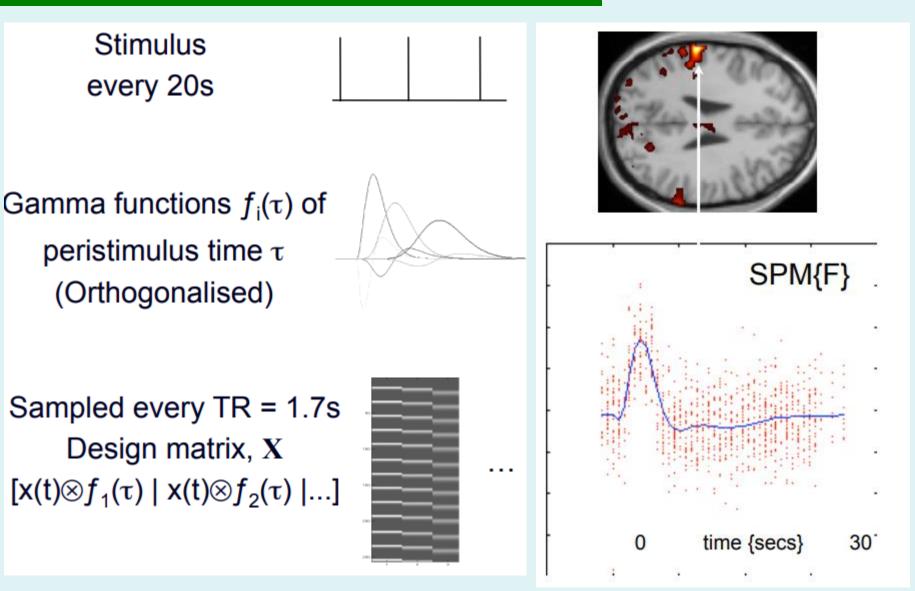
 $f_i(\tau)$ = temporal basis functions

$$y(t) = \sum \sum \beta_i f_i(t - nT) + \varepsilon(t)$$

 $y = XB + \varepsilon$

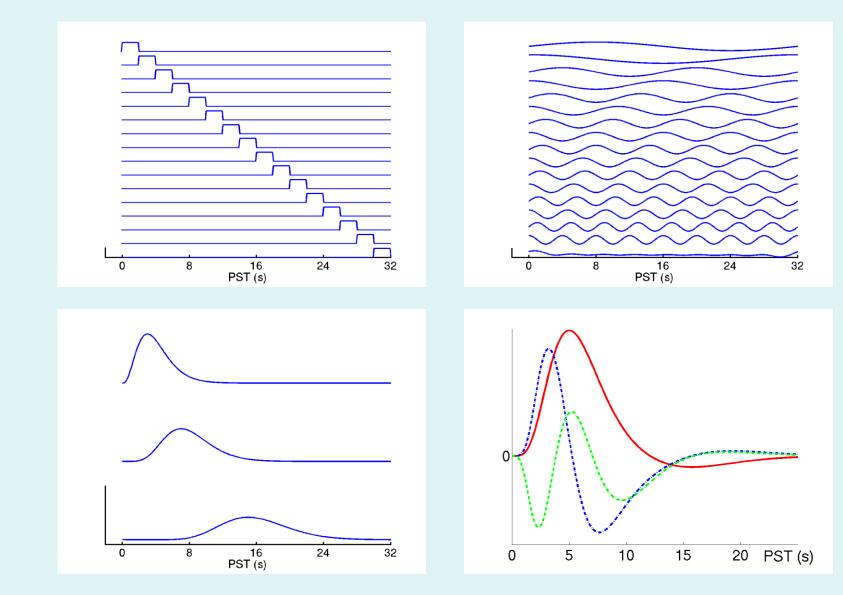


General Linear Model in SPM



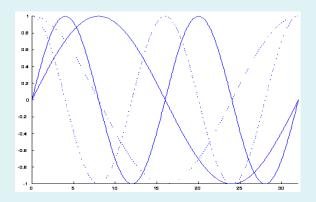
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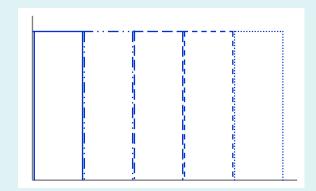
• Fourier Set

Windowed sines & cosines Any shape (up to frequency limit) Inference via F-test



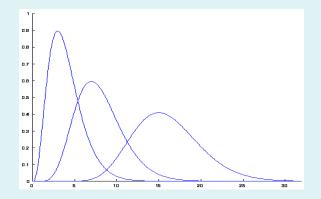
Finite Impulse Response (FIR)

Mini timebins (selective averaging) Any shape (up to bin-width) Inference via F-test



• Gamma Functions

Bounded, asymmetrical (like BOLD) Set of different lags Inference via F-test



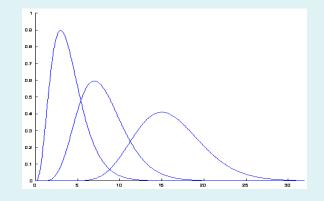
• Gamma Functions

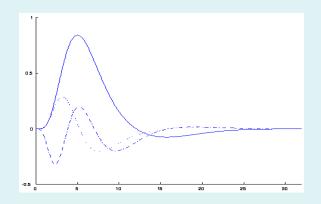
Bounded, asymmetrical (like BOLD) Set of different lags Inference via F-test

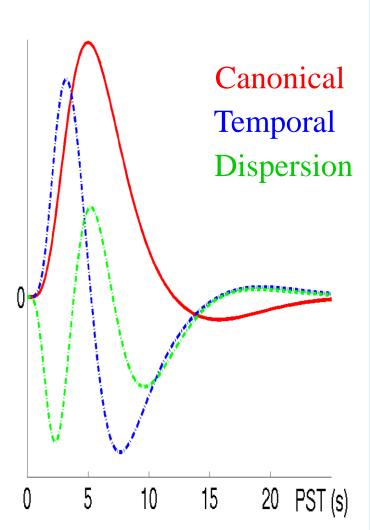


• Informed Basis Set

Best guess of canonical BOLD response Variability captured by Taylor expansion "Magnitude" inferences via t-test...?







Informed Basis Set

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(Friston et al. 1998)
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Canonical HRF (2 gamma functions)

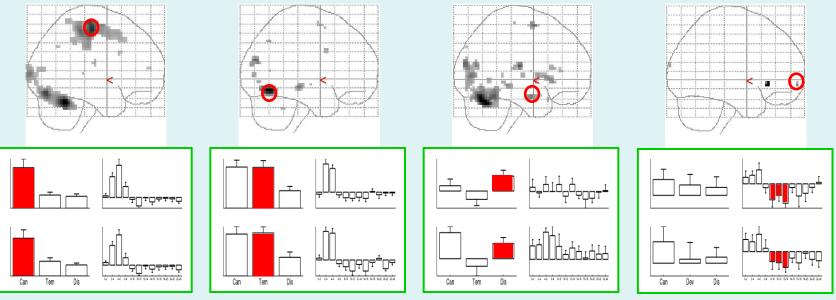
plus Multivariate Taylor expansion in: time (*Temporal Derivative*)

width (Dispersion Derivative)

- "Magnitude" inferences via ttest on canonical parameters (providing canonical is a good fit...more later)
- "Latency" inferences via tests on *ratio* of derivative : canonical parameters (more later...)

Temporal Basis Functions, which one(s)?

In this example (rapid motor response to faces, Henson et al, 2001)...



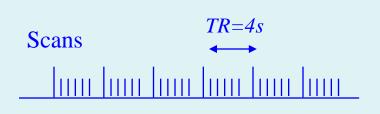
Canonical + Temporal + Dispersion + FIR

...canonical + temporal + dispersion derivatives appear sufficient ...may not be for more complex trials (eg stimulus-delay-response) ...but then such trials better modelled with separate neural components (ie activity no longer delta function) + constrained HRF (Zarahn, 1999)

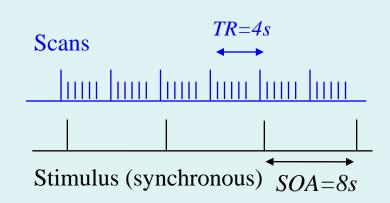
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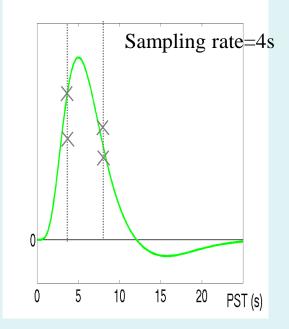
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• Typical TR for 48 slice EPI at 3mm spacing is ~ 4s

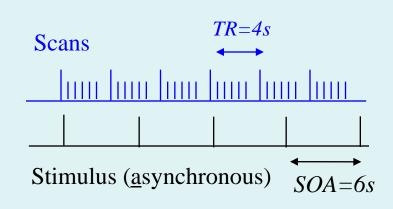


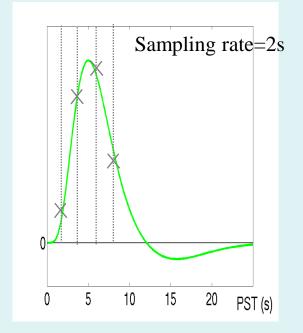
- Typical TR for 48 slice EPI at 3mm spacing is ~ 4s
- Sampling at [0,4,8,12...] post- stimulus may miss peak signal



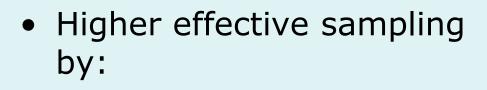


- Typical TR for 48 slice EPI at 3mm spacing is ~ 4s
- Sampling at [0,4,8,12...] post- stimulus may miss peak signal
- Higher effective sampling by:
 - 1. Asynchrony, *e.g. SOA=1.5TR*

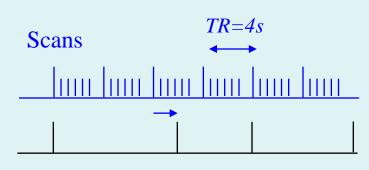




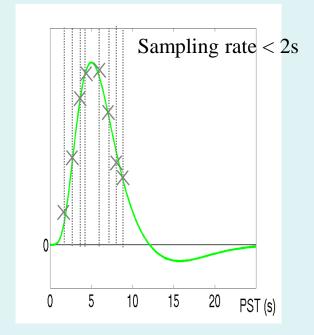
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- 1. Asynchrony, *e.g. SOA=1.5TR*
- 2. Random Jitter, e.g. $SOA = (2 \pm 0.5)TR$



Stimulus (random jitter)



BOLD Response Latency (Linear)

 Assume the real response, r(t), is a scaled (by α) version of the canonical, f(t), but delayed by a small amount dt:

 $r(t) = \alpha f(t+dt) \sim \alpha f(t) + \alpha f'(t) dt$ 1st-order Taylor

• If the fitted response, *R*(*t*), is modelled by the canonical + temporal derivative:

 $R(t) = \beta_1 f(t) + \beta_2 f'(t)$

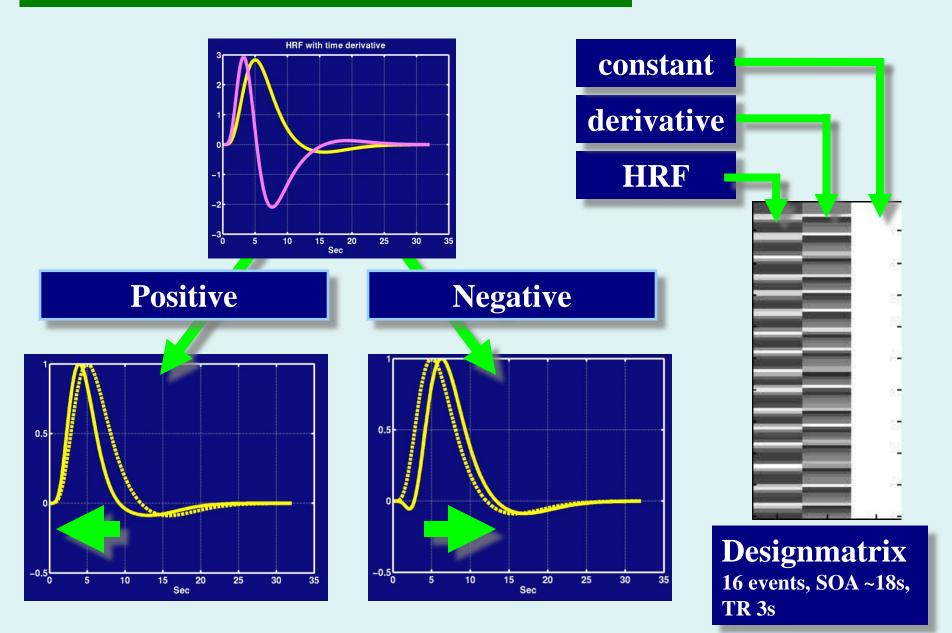
GLM fit

• Then canonical and derivative parameter estimates, β_1 and β_2 are such that:

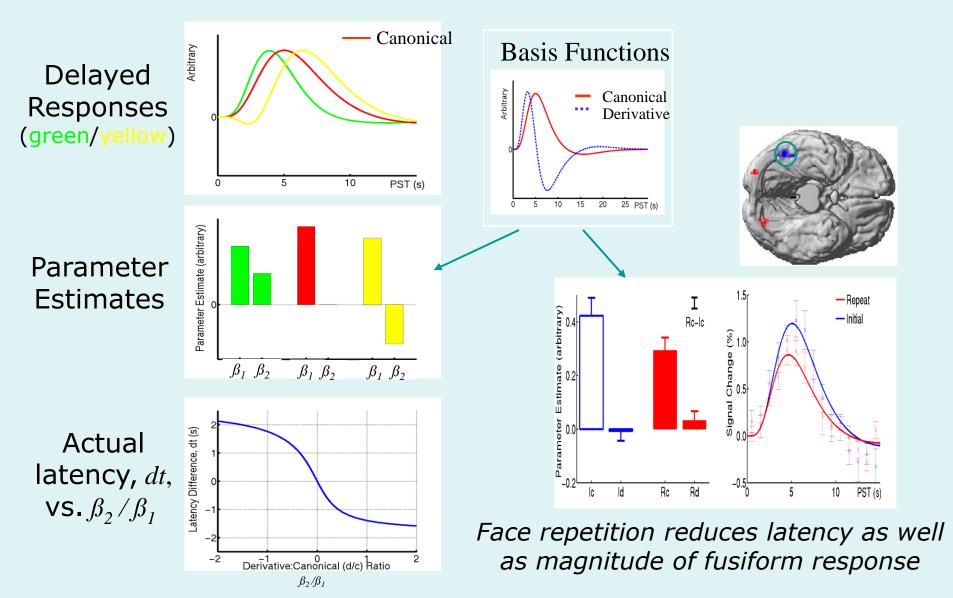
 $\alpha = \beta_{1}, dt = \beta_2 / \beta_1$

• *i.e. latency can be approximated by the ratio of derivativeto-canonical parameter estimates (within limits of firstorder approximation, +/- 1s)*

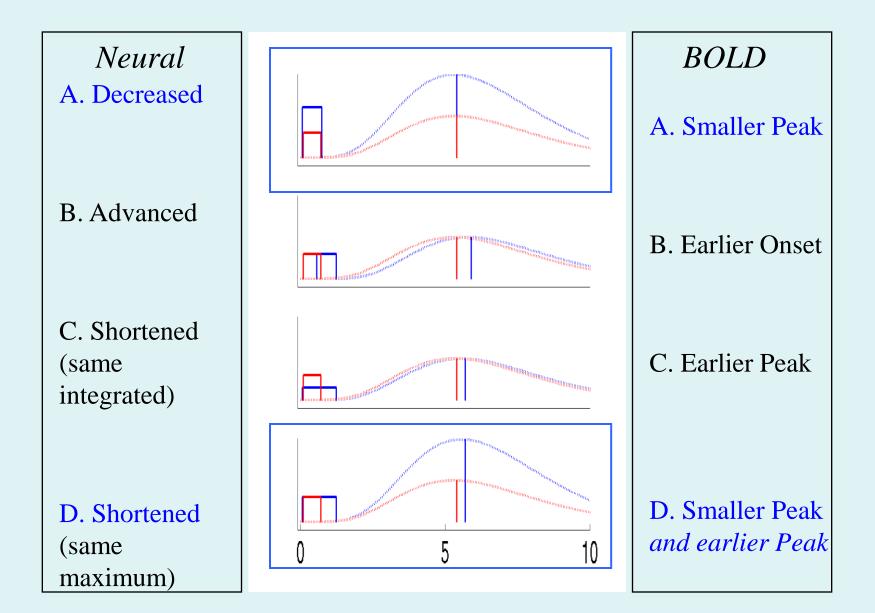
BOLD Response Latency: example



BOLD Response Latency (Linear)



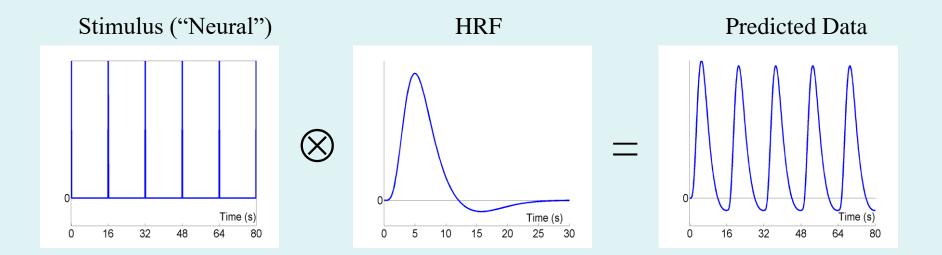
Neural Response Latency



Content

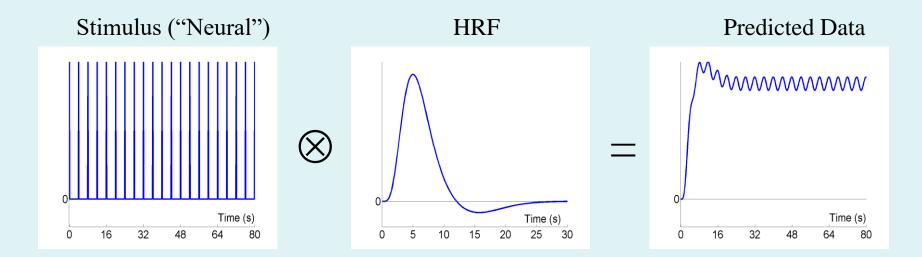
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Fixed SOA = 16s



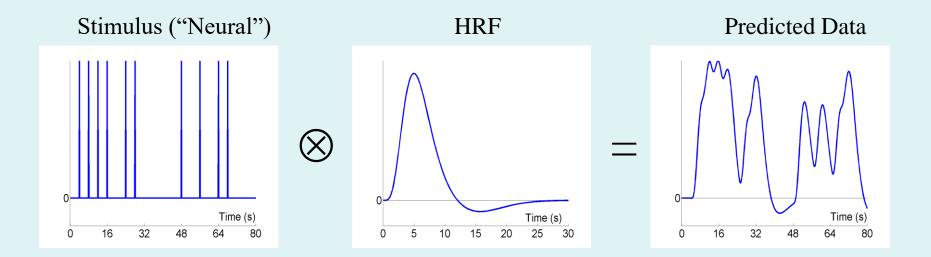
Not particularly efficient...

Fixed SOA = 4s



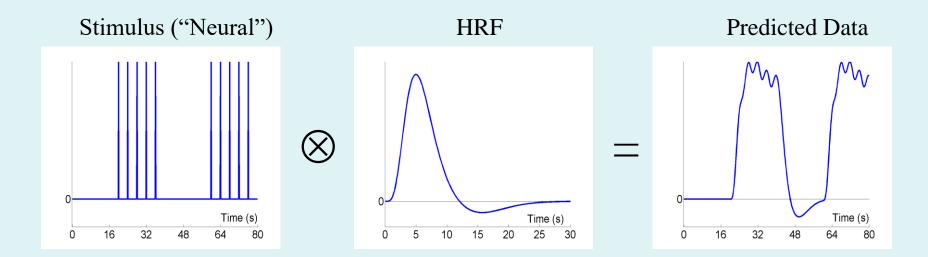
Very Inefficient...

Randomised, $SOA_{min} = 4s$



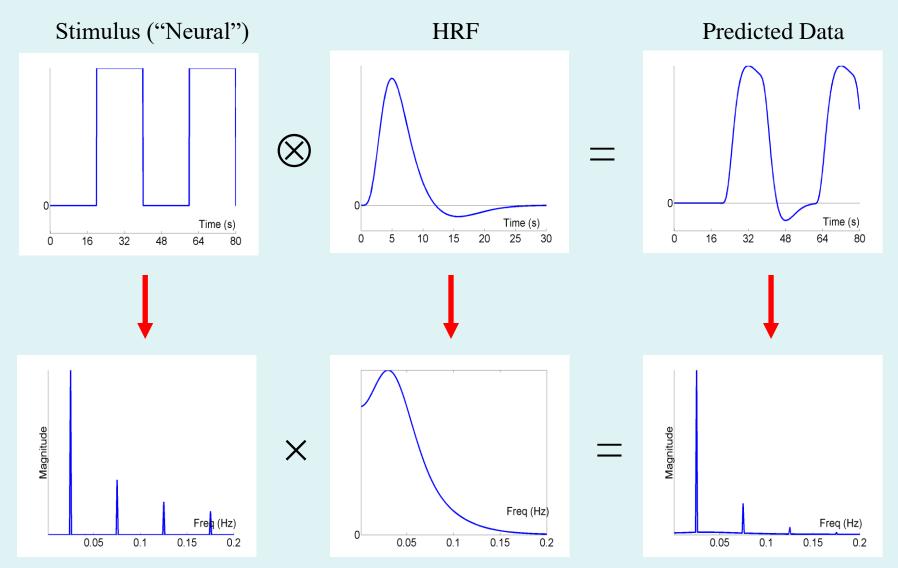
More Efficient...

Blocked, $SOA_{min} = 4s$



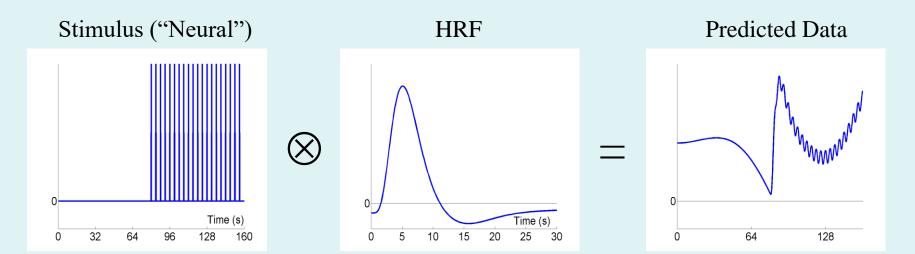
Even more Efficient...

Blocked, epoch = 20s

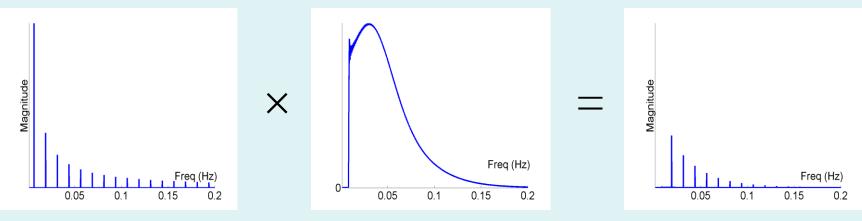


Blocked-epoch (with small SOA) and Time-Freq equivalences

Blocked (80s), SOA_{min} =4s, highpass filter = 1/120s

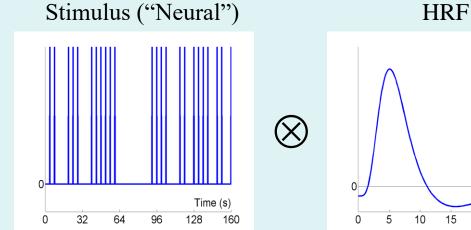


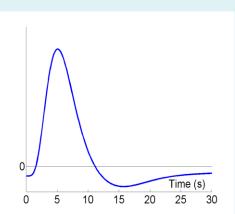
"Effective HRF" (after highpass filtering) (Josephs & Henson, 1999)

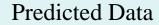


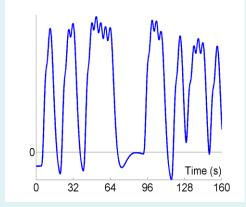
Don't have long (>60s) blocks!

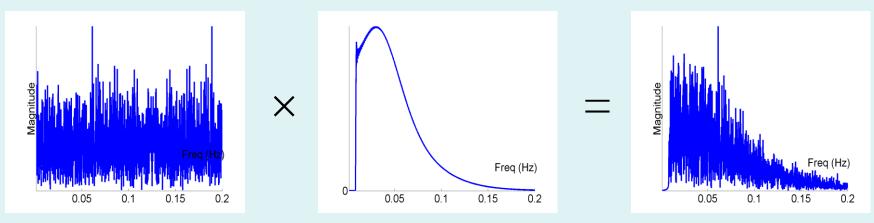
Randomised, SOA_{min} =4s, highpass filter = 1/120s











(Randomised design spreads power over frequencies)

Design Efficiency

Maximise efficiency by maximising t, by minimising the squared variance:

$$t = \frac{c^T \beta}{\sqrt{\operatorname{var}(c^T \beta)}}$$

X: design matrixc: contrast vectorβ: beta vector

Assuming that the error in our model is 'iid', each observation is drawn independently from a Gaussian distribution:

 $b \sim N(b(S^{2}(X^{T}X)^{-1}))$ $\operatorname{var}(c^{T}b) = S^{2}c^{T}(X^{T}X)^{-1}c$

Assuming σ is independent of our design, taking a fixed contrast we can only alter our design matrix to improve efficiency.

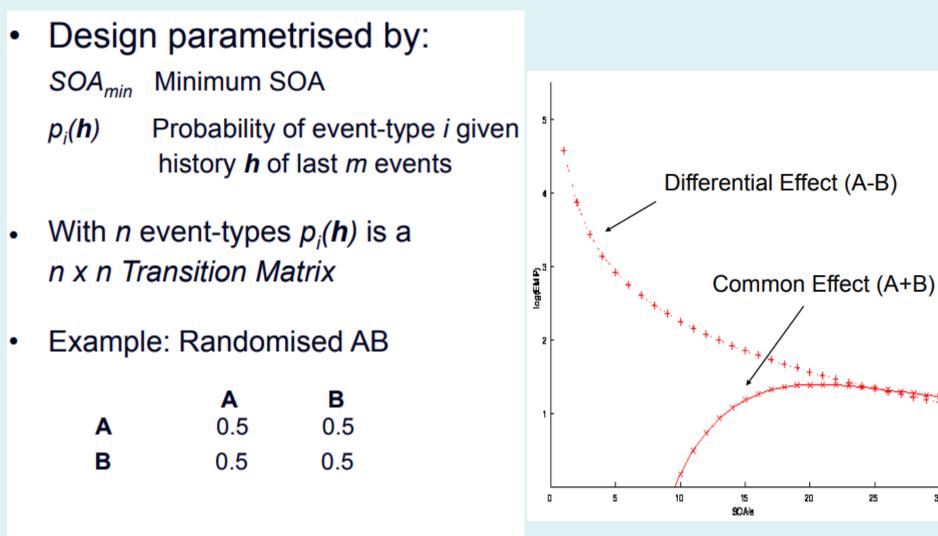
Formal definition of **design efficiency** *e* » minimises variance:

$$\frac{1}{\sqrt{c^T (X^T X)^{-1} c}}$$

Given the contrast of interest, minimise covariance in the design matrix

Efficiency can be estimated before using the design

Design efficiency: Trial sequencing



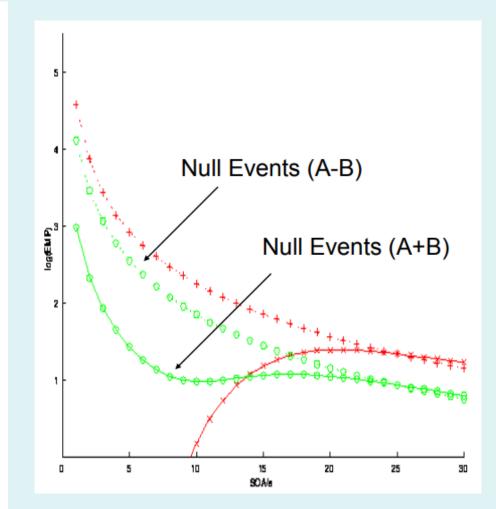
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Design efficiency: Trial sequencing

• Example: Null events

ABA0.330.33B0.330.33

- => AB-BAA--B---ABB...
- Efficient for differential and main effects at short SOA
- Equivalent to stochastic SOA (Null Event like third unmodelled event-type)



Design efficiency: Trial sequencing

- Example: Alternating AB
- В Α 5 Α 0 В 0 Permuted (A-B) => ABABABABABAB... Alternating (A-B) log(EMP) 22 • Example: Permuted AB В Α ¥ * * * AA 0 AB 0.5 0.5 BA 0.5 0.5 BB O 10 5 20 25 П 15 SOAla => ABBAABABABBA...

30

Design efficiency: Conclusions

- Optimal design for one contrast may not be optimal for another
- Blocked designs generally most efficient (with short SOAs, given optimal block length is not exceeded)
- However, psychological efficiency often dictates intermixed designs, and often also sets limits on SOAs
- With randomised designs, optimal SOA for differential effect (A-B) is minimal SOA (>2 seconds, and assuming no saturation), whereas optimal SOA for main effect (A+B) is 16-20s

Design efficiency: Conclusions

- Inclusion of null events improves efficiency for main effect at short SOAs (at cost of efficiency for differential effects)
- If order constrained, intermediate SOAs (5-20s) can be optimal
- If SOA constrained, pseudorandomised designs can be optimal (but may introduce context-sensitivity)

